

SHORT REPORT

Control of Movement

Rapid responses to reach errors are equally strong during fixation and visual pursuit

 Renato Moraes,^{1,2*}  Jolande Fooker,^{2,3*} Jason P. Gallivan,^{2,4} and  J. Randall Flanagan²

¹School of Physical Education and Sport of Ribeirão Preto, University of São Paulo, Ribeirão Preto, Brazil; ²Department of Psychology and Centre for Neuroscience Studies, Queen's University, Kingston, Ontario, Canada; ³Department of Psychology and Centre for Cognitive Science, Technical University Darmstadt, Darmstadt, Germany; and ⁴Department of Biomedical and Molecular Sciences, Queen's University, Kingston, Ontario, Canada

Abstract

When reaching to a foveated target, peripheral vision of the hand can be used to make rapid, automatic adjustments to the ongoing reach movement, with feedback gain being sensitive to features of the task and environment. These rapid corrective responses are also observed when gaze is directed to a stationary “gaze” target located away from the reach target. In everyday contexts, reaching often occurs concurrently with other visual or visuomotor tasks, such as tracking a moving target. Yet it remains unclear whether engaging in such tasks affects the use of peripheral vision for hand guidance. Here, we compare rapid visuomotor corrective responses to visual perturbations during fixation and smooth pursuit, and test whether pursuit-related and reach-related visuomotor processes operate independently or compete for shared visual resources. Participants either fixated a stationary target or tracked a moving target while reaching toward a spatially dissociated reach target. During the reach, the visual representation of the hand was perturbed, requiring rapid corrective responses. We found that neither the onset nor the gain of reach corrections was modulated by gaze-task demands. Moreover, response gains were strongly correlated across tasks, indicating consistent individual response profiles that were independent of the gaze condition. Although participants remained engaged in the smooth pursuit task, their performance slightly declined during reaching compared with the preparatory period. Together, these findings demonstrate that rapid, automatic visual feedback mechanisms during reaching are equally robust during pursuit tracking and fixation of a separate gaze target.

NEW & NOTEWORTHY In everyday life, reaching an object can occur while the eyes are engaged in competing visual tasks. We show that engaging in smooth pursuit eye movements does not disrupt rapid visuomotor corrections during reaching. Corrective response gain following perturbation was unchanged by gaze-task demands, although pursuit performance slightly deteriorated during reaching. These findings indicate that rapid visuomotor processes engaged when reaching a target are independent of whether gaze is fixating or pursuing a separate target.

feedback gain; gaze; peripheral vision; reaching movements; sensorimotor integration

INTRODUCTION

Visuomotor control in reaching involves integrating visual information with motor commands to accurately move the hand toward a target location. To effectively use peripheral vision and gaze-related signals—including gaze proprioceptive signals—in reaching, individuals typically fixate the

target throughout the reaching movement (1–3). These visual signals can be used to correct for movement errors following hand or target perturbation. Such reach corrections are characterized by a quick correction onset (80–150 ms) and flexible feedback gain, i.e., the magnitude of the corrective response (4). Whereas the onset of reach corrections occurs automatically and independently of features in the visual



*R. Moraes and J. Fooker contributed equally to this work.
Correspondence: R. Moraes (renatomoraes@usp.br).
Submitted 5 March 2026 / Revised 23 March 2026 / Accepted 8 May 2026



environment, feedback gains are sensitive to task context and goal (5–9).

In real-world situations, goal-directed reaching may occur in parallel with a competing visual or visuomotor task, such as identifying objects, monitoring environmental events, or tracking a moving object. Past research has shown that the visuomotor coordination, including corrective responses, remains intact when individuals fixate a “gaze target” located away from the reach goal (10–14). However, it is unknown whether engaging in a more complex visual task, in which the eye position changes dynamically, influences our ability to use peripheral vision and gaze-related signals to direct the hand.

The aim of this study is to determine whether engaging in an ocular tracking task affects our ability to use gaze-related signals to direct and correct hand movements toward a peripheral reach target. We developed a task in which participants moved a cursor, displayed on a vertical monitor, from a start position to a reach target by moving the handle of a robotic manipulandum in the horizontal plane. In two conditions, participants either fixated a stationary gaze target (fixation condition) or tracked a moving gaze target (pursuit condition) prior to and during the reach movement. To assess the efficacy of the visuomotor control in reaching, we measured the onset and gain of the rapid visual feedback responses (mismatches between actual and predicted sensory feedback). Specifically, we included perturbation trials in which we jumped the cursor position to the left or right while it passed beneath an occluder (3, 15, 16), and measured the gain of the resulting rapid corrective response using a force channel (9–11, 17, 18).

Our paradigm allows us to address two alternative hypotheses. First, engaging in the ocular tracking task might interfere with the ability to use visuomotor signals to correct movement errors. Here, we would expect the timing and gain of the visuomotor corrective response to differ between the fixation and pursuit conditions. This would suggest that the two tasks operate dependently and thus visual resources cannot be fully used in parallel. Alternatively, performing the ocular-tracking task might not interfere with the visuomotor control of reaching. Here, we would predict that individuals can effectively integrate peripheral visual information and gaze-related signals to produce rapid, automatic corrective responses to visual perturbations, even while tracking a moving gaze target. Thus, the gain and onset of correction of these visuomotor feedback responses should be comparable in the pursuit and fixation conditions. This would suggest that ocular pursuit and reach-related visuomotor processing can operate in parallel without interference, indicating a degree of independence between these visuomotor functions.

MATERIALS AND METHODS

Participants

Twenty-four adults (21.7 ± 5.2 yr, 16 women, 23 right-handed) participated in this study. Previous studies that investigated automatic reaching adjustments using force channels typically included 8–15 participants (9, 11, 17, 18). We therefore targeted a larger sample to obtain more

informative evidence for or against the null hypothesis. Queen’s University students received one course credit, and community members outside the university received \$15 for their participation. All participants had normal or corrected-to-normal vision, no upper-limb limitations, and no neurological conditions. The session lasted about 1 h, and all participants provided written consent. The study was approved by the Queen’s University Research Ethics Committee. Data from four participants were excluded due to eye-tracker calibration issues and one due to possible nystagmus, resulting in a final sample of 19 participants (21.6 ± 5.2 yr; 13 women; 18 right-handed).

Apparatus

Participants operated a KINARM end point robotic manipulandum (BKIN Technologies, Kingston, ON, Canada) that allowed horizontal plane movements to control a cursor on a vertical plane monitor (70 × 39.5 cm; 1,920 × 1,080 resolution; 60 Hz). The timing of when the cursor exited the occluder (see *Procedure*) was corrected for display delay, using the latency reported by the graphics card and the estimated refresh latency (~50 ms). The mapping between the robotic handle and the cursor resembled that of a standard computer mouse: moving the handle forward or to the right moved the cursor upward or to the right. Kinematic data and force data were sampled at 1,000 Hz. During the task, right eye movements were recorded using a monocular Eyelink 1000 system (SR Research Ltd., Kanata, ON, Canada) at 500 Hz.

Visual Stimuli

The hand position was represented on the screen as a circular cursor (1 cm in diameter) aligned with the handle of the robotic manipulandum. A 1-cm visual stimulus was equivalent to 1.5 visual degrees. Movements were made from a circular initial position (1 cm in diameter) to a circular target area (2 cm in diameter) located 25 cm above the initial start position (Fig. 1A). A 15 × 5 cm occluder was positioned between the start position and the target so that the far edge of the occluder was at the midpoint of the required reaching movement (i.e., 12.5 cm from the start position). Two visual targets were used to test how corrective responses depended on visual tasks: fixation (stationary gaze target) and smooth pursuit (moving gaze target). Participants had to maintain their gaze on the gaze target region throughout the trial so that the reaching movement was guided by peripheral vision (Fig. 1A). In the stationary gaze target, participants looked at a circular fixation target (0.5 cm diameter) (Fig. 1E). In the moving gaze target, participants were asked to track the displacement of the dot with their eyes as accurately as possible. The trajectory of the dot’s displacement was defined by equations described in previous studies (19, 20). All trajectories had a period t of 6.3 s (fundamental frequency $\omega = 1$ Hz; $t = 2 \times \pi/\omega$). The parameters used to generate the trajectories were replicated from a previous study (21).

Procedure

Participants adjusted the seat height, positioned their chin and forehead on the support, and then completed the eye-tracker calibration. They first completed a familiarization

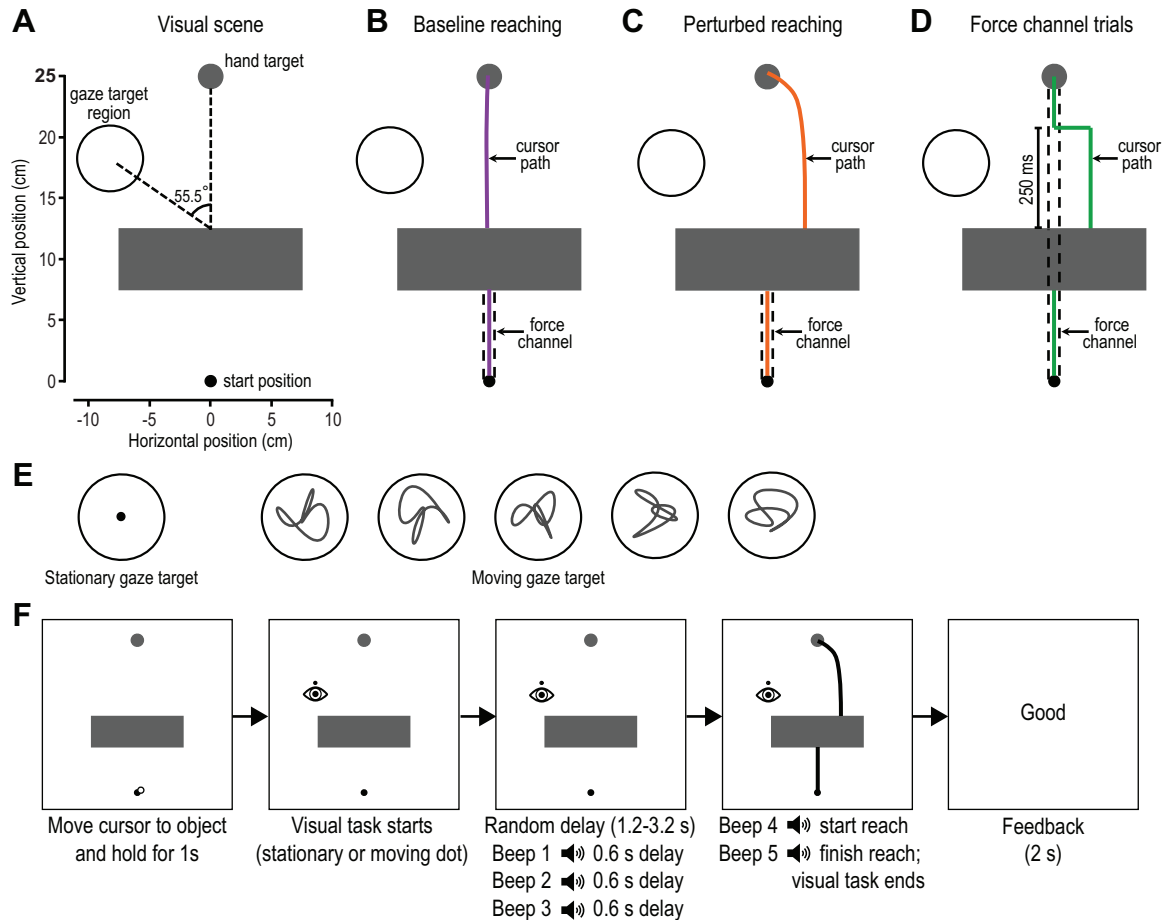


Figure 1. Experimental setup and conditions. *A*: two-dimensional (2-D) view of the visual scene centered at the start position. The start position was represented by an object (an empty circle with a diameter of 1 cm). For the visual task, participants either fixated a stationary circle (stationary gaze target) or tracked a dot that could move (moving gaze target) within the circle located in the left region (which was not shown to participants). The stationary gaze target was positioned at the centered coordinates $x = -8$ cm and $y = 18$ cm. Relative to the center of the farthest edge of the occluder, this location placed the target 55.5° away at a distance of 9.7 cm. *B*: illustration of a trial without perturbation (baseline reaching). Participants performed the reaching movement from the starting position to the target while fixating the gaze target with their eyes. *C*: illustration of a perturbation trial without a force channel following the perturbation (perturbed reaching). In these trials, the hand cursor was visually perturbed by shifting it 3 cm to the left or right after passing under the visual occluder. *D*: illustration of perturbation and force channel trial. In this condition, participants' movements were constrained to move along a straight line from the start position to the target, allowing measurement of the forces applied to the virtual walls of the force channel (dashed lines). The cursor automatically returned to the straight line 250 ms after the perturbation onset in these trials. *E*: illustration of the stationary gaze target (*left side*) and the five dot trajectories used in the moving gaze target condition. *F*: temporal sequence of events in each trial. After the visual scene was presented, participants had to move the cursor to pick up the object. The visual task started 1 s after the object was “picked up.” The interval between beeps was fixed (0.6 s), and participants were instructed to begin to reach at the same time as beep 4 and finish the reach at the time of beep 5. After completing the reaching task, participants received feedback about the duration of the reaching movement.

block of 36 trials, divided equally between stationary and moving gaze targets; for the moving condition, only trajectory 1 was used (Fig. 1E). Within this block, there were 12 nonperturbed, 12 perturbed, and 12 force-channel trials, presented in a pseudo-randomized order. To facilitate familiarization, the first 10 trials were fixed: 5 nonperturbed trials with a stationary gaze target, followed by 5 nonperturbed trials with a moving gaze target. The remaining trials (including all conditions) were then randomized. This sequence ensured gradual familiarization with the tasks.

General task.

Once the visual scene appeared (object, target, and occluder), participants moved the cursor to the initial position to pick up the object and held it there (Fig. 1F). After 1 s, the dot for

the gaze target task appeared. After a delay between 1.2 and 3.2 s, five successive beeps (400 Hz; 80 ms) were presented 600 ms apart. The beeps served as a go cue: participants were instructed to start reaching on the fourth beep and arrive at the target on the fifth beep. On all trials, the cursor passed under the occluder. In perturbation trials, the cursor jumped 3 cm left or right below the occluder, requiring corrective adjustments when it reappeared to hit the target. The trial ended once the center of the cursor remained in the target for 300 ms. After each trial, a central message on the screen displayed movement time feedback (“good,” “very fast,” or “very slow”) to encourage consistent timing across trials and participants (9–11). Movement time from 1 cm above the initial position until 1 cm below the target was considered good between 400 and 700 ms (9–11). Participants

were instructed to adjust their speed when feedback indicated it was not “good.” Trials outside this range were excluded (251 trials; 8.8% of 2,850 total trials). Considering only channel trials, 39 (6.8%) and 48 (8.4%) of 570 trials were excluded in the stationary and moving gaze target conditions, respectively.

Non-perturbed reaching.

In this condition, only the first 7.5 cm of movement was restricted by a mechanical channel (stiffness 2,000 N/m, damping 0.2 N/m/s) (Fig. 1B). The mechanical channel parameters were lower than those used in our previous work (stiffness 6,000 N/m, damping 1.5 N/m/s) (10, 11), but yielded response gains similar to or greater than those previously reported, indicating that these parameters were adequate to capture response gain. This restricted the initial reach to a straight line up to the near edge of the occluder and ensured that the cursor exited the occluder close to the line connecting the initial position and the target center (10, 11).

Perturbed reaching.

As in nonperturbed reaching, only the first 7.5 cm of movement was restricted by the mechanical channel (Fig. 1C). In this condition, the cursor jumped under the occluder and reappeared 3 cm to the right or left of the line between the start position and the hand target (10, 11). Participants then had to correct the cursor’s trajectory to reach the hand target.

Force channel trials.

We used force channel trials to assess the gain of corrective responses. In these trials, handle movement was restricted along a straight path from the initial position to the hand target position by a mechanical channel generated by the robot (Fig. 1D), allowing us to measure corrective forces exerted on the channel wall following visual perturbations. In these trials, the cursor exited the occluder either 3 cm to the left or right and was automatically shifted back to the straight path 250 ms after perturbation onset, consistent with previous work (9–11, 17, 18). Because this change occurred near the time of correction, participants typically believed they were responsible for returning the cursor to the target. To avoid adaptive reductions in response magnitude, only 40% of trials used the force channel, randomly interspersed with non-channel trials.

Participants completed 15 trials for each of 10 experimental conditions: 2 perturbation directions (–3 cm [left] and +3 cm [right]) × 2 gaze tasks (stationary and moving) × 2 force channel conditions (without [perturbed reaching] and with [force channel trials]), totaling 8 conditions (120 trials). The two remaining conditions combined both gaze tasks with the nonperturb reaching, totaling 30 trials. All 150 trials were evenly distributed across 3 blocks in a single session, with trial order randomized within each block. Participants rested between blocks as needed to prevent fatigue. The experiment lasted ~1 h.

Data Analysis

Eye and hand movement data were analyzed offline using custom MATLAB routines (v.2020b). Hand movements were

examined using the *x*- and *y*-positions of the robotic handle, filtered with a low-pass third-order Butterworth filter (cutoff = 10 Hz). Eye movements were analyzed from calibrated screen-centered *x*- and *y*-coordinates, filtered with a second-order low-pass Butterworth filter (cut-off = 15 Hz) and resampled to 1,000 Hz. Filtered data were used to identify fixations and gaze shifts.

The hand, dot, and gaze signals were differentiated to obtain velocity traces. Hand and gaze velocities were then low-pass filtered (10 and 25 Hz, respectively) to reduce noise from numerical differentiation. Hand onset was defined as the moment the vertical hand velocity first exceeded 5% of its peak value obtained during the reaching movement.

Force channel trials.

To obtain a measure of the strength of corrections in response to cursor displacement (i.e., response gain), lateral forces in force channel trials were averaged over 180–230 ms after perturbation onset (9–11, 18). For each participant and condition, the mean force following a leftward perturbation was subtracted from that following a rightward perturbation to obtain the corrective force difference (corrective force amplitude), computed separately for each gaze task. To assess whether stimulus location biased gain values toward the left, we conducted a two-way ANOVA (perturbation side [left, right] and condition [stationary, moving]). No evidence of a leftward bias was found (perturbation side: $P = 0.178$; condition: $P = 0.545$; interaction: $P = 0.715$). To calculate the onset times of force corrections, we compared individual force traces for left and right perturbations within each condition. Paired *t* tests were applied at each time point after the perturbation onset to obtain the minimum *P* value, then searched backward to locate the first time point with $P < 0.001$, which defined the onset of correction.

Visual task.

Eye-position error was calculated as the root-mean square error during fixation and smooth pursuit. This was obtained by subtracting the dot coordinates from the gaze coordinates. Visual gain between eye and gaze target velocities was computed for the moving gaze target task. Resultant velocities for both eye and gaze targets were calculated from their *x*- and *y*-velocity components. Eye velocity gain was calculated by dividing eye velocity (with catch-up saccades removed) by gaze target velocity.

Participants exhibited poor fixation or pursuit in some trials, characterized by large saccades that displaced the eyes significantly from the gaze target. Based on previous work (22), a 6-cm diameter boundary was defined around the center of the gaze target region (Fig. 2, A and B). Trials in which saccades landed outside this boundary were excluded (140 trials; 4.9% of 2,850 total trials). Trials were included in the analysis only if saccades remained within the defined boundary throughout the trial. Considering only channel trials, 23 (4.0%) and 19 (3.3%) of 570 trials were excluded in the stationary and moving gaze target conditions, respectively. Across both exclusion criteria (movement time and saccade location), 11.3% of channel trials were removed from the analysis.

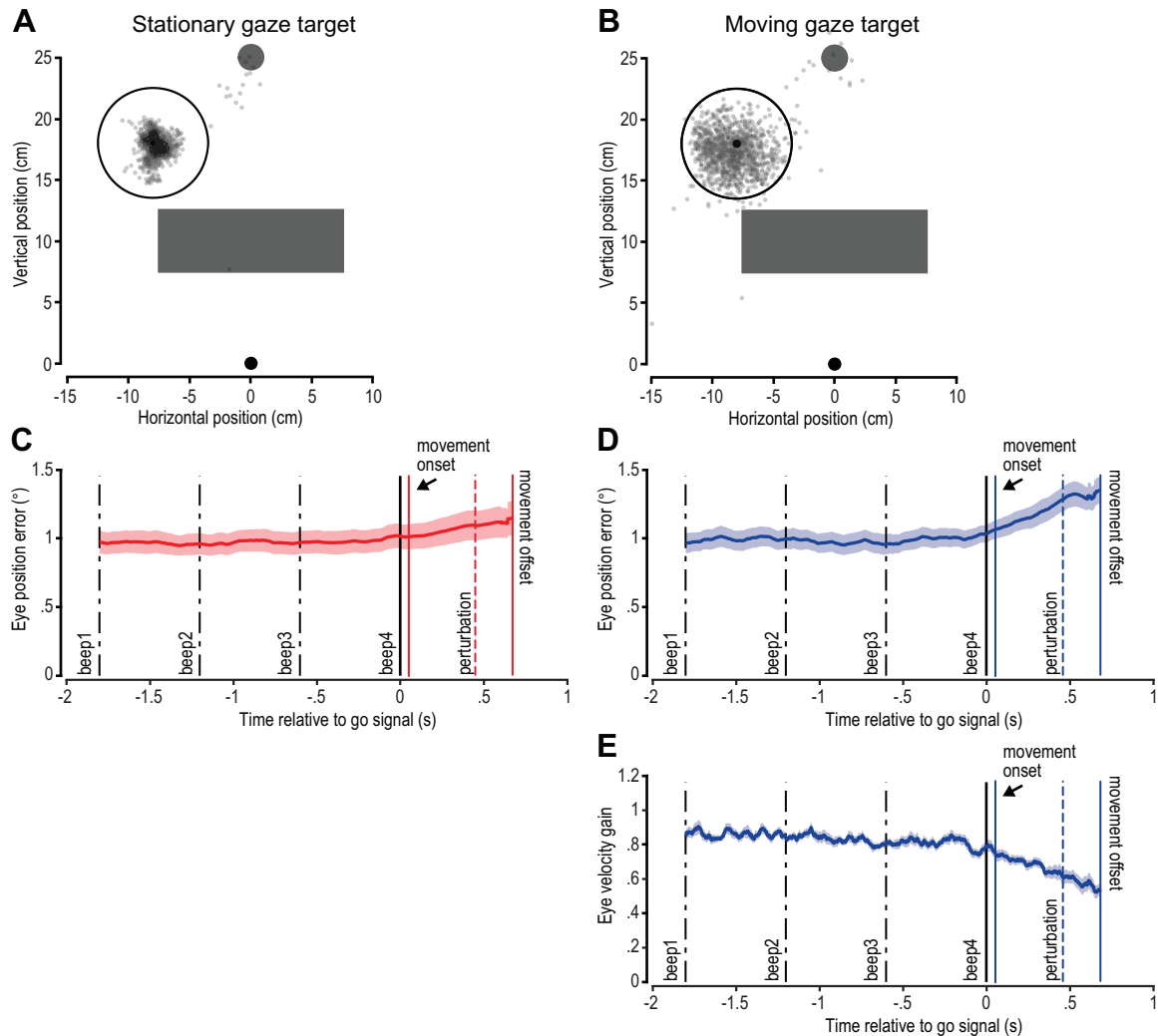


Figure 2. Eye position and saccade endpoints during reaching movements toward stationary and moving gaze targets for the channel trials. **A:** in the stationary gaze target task, the saccade endpoints are shown in the *top* as gray dots. Trials in which saccades landed more than 6 cm away from the gaze target zone (continuous circle on the left side) were excluded from analysis (see MATERIALS AND METHODS). **B:** the layout in the moving gaze target condition is similar to that in (A). The dark gray rectangle represents the occluder in (A and B). **C and D:** eye position error averaged across trials and participants for the stationary (C) and moving (D) gaze targets. **E:** eye velocity gain averaged across trials and participants for the moving gaze target. For C, D, and E, the data are aligned to beep 4, and the shadow region around the mean corresponds to one standard error.

Statistical Analysis

Statistical analyses were performed in JASP (23). Statistical tests performed are described throughout RESULTS. In the text, results are presented as means (M) and standard errors (SE; $M \pm SE$). The significance level was $P < 0.05$.

RESULTS

Participants Can Perform a Secondary Gaze Task during Reaching

Participants were instructed to fixate on the gaze target during stationary trials or pursue it during moving trials. Figure 2, A and B, shows all saccade endpoints (gray dots) for stationary and moving conditions. Participants generally kept their gaze within the 6-cm boundary, though occasional large saccades occurred toward the hand target or elsewhere.

Figure 2, C and D, shows the average gaze position error, based on participant medians, as a function of time, for stationary and moving gaze targets, and Fig. 2E shows the average eye velocity gain, based on participant medians, as a function of time for the moving gaze target. Participants clearly maintained fixation on the stationary gaze target, and pursuit of the moving gaze target, during the entire trial. In the pursuit condition, gaze error increased slightly and eye velocity gain decreased slightly during the reach. To quantify these effects, we compared the period of time between the second and third beeps (baseline) to the period of time between movement onset and offset. In the moving condition, the gaze error during the reach ($1.19^\circ \pm 0.08^\circ$) was greater ($t_{18} = 4.2$, $P < 0.001$, $d = 0.966$) than during baseline ($0.97^\circ \pm 0.07^\circ$), and the eye velocity gain during the reach (0.76 ± 0.03) was smaller ($t_{18} = 7.6$, $P < 0.001$, $d = 1.746$) than during baseline (0.97 ± 0.02). In the stationary condition,

there was no significant difference ($t_{18} = 2.1, P = 0.053, d = 0.475$) in the gaze error during baseline ($0.96^\circ \pm 0.08^\circ$) and reach ($1.05^\circ \pm 0.10^\circ$).

Hand Movement Kinematics Are Independent of Gaze Task Demands

Hand kinematic parameters were similar between the stationary and moving gaze targets, indicating that the moving visual cue had minimal influence on the timing or kinematics of the reaching movement (Fig. 3). Figure 3A shows cursor (i.e., hand) displacement in nonchannel trials, where participants moved straight forward in both gaze conditions without perturbation. After left or right perturbations, trajectory adjustments appeared near the end of the reaching movement. The cumulative plots show data from the force channel trials (Fig. 3, B–D). Kolmogorov–Smirnov tests revealed no significant difference between gaze conditions for any hand-movement parameter (vertical hand peak velocity: $P = 0.609$; movement duration: $P = 0.559$; movement onset relative to 4th beep: $P = 0.688$). On average, vertical hand peak velocity was 62.6 ± 0.2 cm/s, movement duration was 519 ± 2 ms, and reaching movement started 91 ± 7 ms after beep 4. Peak hand velocity occurred, on average, 12 ± 4 ms before the cursor left the occluder, showing that hand velocity was comparable across conditions around the cursor jump. Moreover, interindividual differences in hand movement kinematics were consistent between gaze target conditions, as indicated by strong correlations for all measures (see the scatterplots shown in Fig. 3, B–D; vertical hand peak velocity: $r = 0.938$; movement duration: $r = 0.794$; movement onset relative to 4th beep: $r = 0.984$; all $P < 0.001$).

We also compared hand movement parameters between nonperturbation and perturbation conditions, using nonchannel, nonperturbed trials to represent the nonperturbation condition (Fig. 3A). Kolmogorov–Smirnov tests again showed no significant differences (vertical hand peak

velocity: $P = 0.060$; movement duration: $P = 0.060$; movement onset relative to the fourth beep: $P = 0.524$).

To assess whether the moving gaze target influenced lateral movement variability, we quantified hand end point variability using the nonchannel and perturbation trials. Endpoint variability was computed as the standard deviation of hand end point positions across trials for each participant in the horizontal (x) and vertical (y) directions. Paired t tests revealed no significant differences between stationary (x -direction: 0.49 ± 0.02 cm, y -direction: 0.45 ± 0.02 cm) and moving (x -direction: 0.53 ± 0.03 cm, y -direction: 0.46 ± 0.03 cm) gaze targets in either the x -direction ($t_{18} = 1.4, P = 0.188, d = 0.314$) or the y -direction ($t_{18} = 0.5, P = 0.646, d = 0.107$). These results indicate that the moving gaze target did not meaningfully affect hand end point variability.

Movement Correction Onset and Gain Are Not Modulated by Gaze-Task Demands

Figure 4, A and B, shows, for the force channel trials, the forces exerted on the channel wall for the left and right perturbations in the two gaze targets for each participant (thin lines) and the averages across participants (thick lines). Figure 4C shows the individual values of the correction onset times of the force responses during the reaching movement to the hand target. Correction onset times ranged from 140 ± 5 ms to 149 ± 4 ms for the stationary and moving gaze targets. The t test for paired samples did not detect a significant difference between the gaze targets ($t_{18} = -2.0, P = 0.057, d = 0.466$). A Bayesian paired t test indicated that the data were 1.277 times more likely under the alternative than the null hypothesis, providing inconclusive evidence for the alternative. In addition, we found no association between gaze target conditions for the correction onset ($r = 0.399, P = 0.090$), as illustrated in the scatterplot (Fig. 4C).

As shown in Fig. 4, A and B, the interval used to calculate the mean force (180–230 ms) represents the period just after

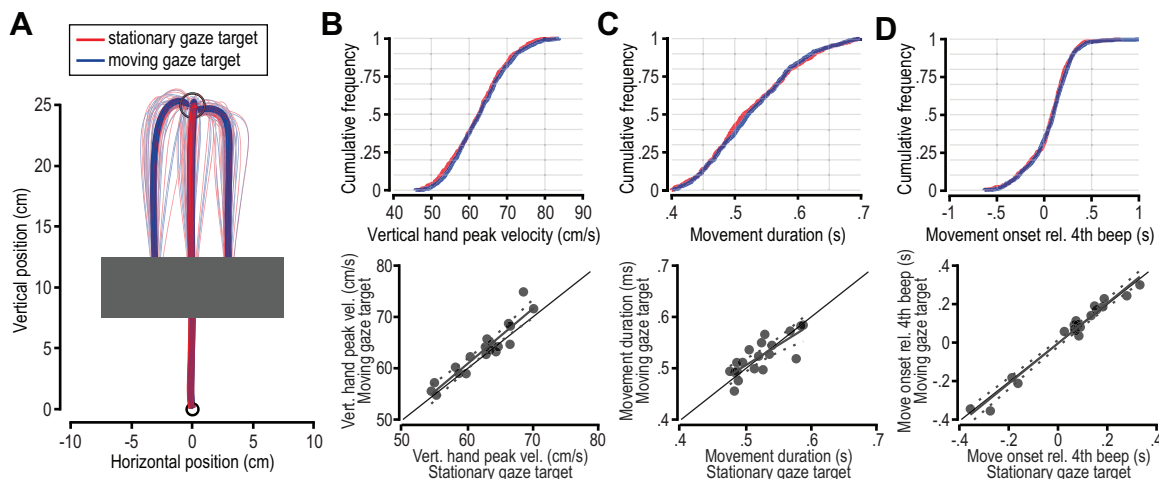


Figure 3. Hand kinematics and timing parameters under stationary and moving gaze targets. A: hand trajectories for each participant (thin lines) and average trajectory (thick lines) for the nonchannel trials in the two gaze target tasks: stationary (red) and moving (blue). The gray shaded area indicates the occluder region. B–D, top: cumulative frequency distributions of vertical hand peak velocity, movement duration, and movement onset time relative to the fourth auditory beep (used as a temporal go signal), respectively, across participants and trials for the channel trials. B–D, bottom: scatterplots between stationary and moving gaze targets for the same variables described at the top. For these scatterplots, the median values of each participant and condition were used. Dashed lines indicate the 95% confidence interval for the line fitted to these data.

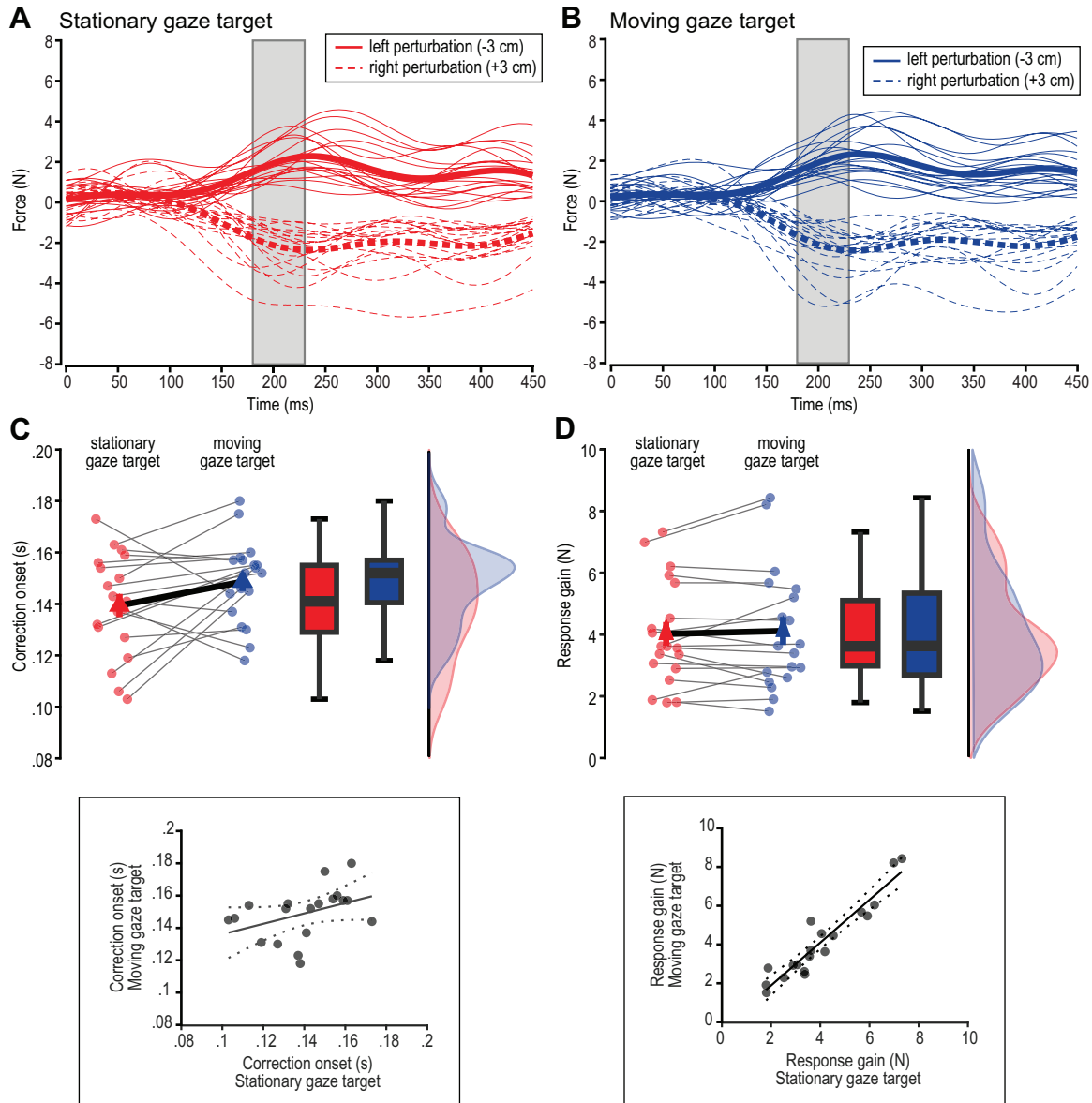


Figure 4. Visuomotor feedback gain and correction onset for stationary and moving gaze targets. Forces measured in force channel trials in the stationary (A) and moving gaze (B) targets. Responses are plotted for leftward (solid) and rightward (dashed) perturbation of the hand cursor during hand target reaching. Thin lines indicate the average forces for each participant, and thick lines indicate the average force across participants. The 0-ms corresponds to the instant of cursor jump. The gray area indicates the 180–230 ms interval used to average the force differences to obtain a single measure of response gain. The mean force values after a leftward cursor perturbation were subtracted from the mean forces after a rightward cursor perturbation to obtain the corrective force difference or response gain. The separation between left and right force time series was used to identify the onset time of correction following the cursor perturbation. C and D, top: the top graph shows the correction onset (C) and the response gain (D) values for each participant (small dots) for both stationary (red symbols) and moving (blue symbols) gaze targets. The triangle indicates the mean, and the vertical bars indicate the standard error. On the right, the boxplots and probability density functions for both gaze targets are shown. C and D, bottom: scatterplots between stationary and moving gaze targets for the same variables described at the top. Dashed lines indicate the 95% confidence interval for the line fitted to these data.

the onset of the response to the perturbation. The response gains were statistically compared using paired *t* tests to examine the effect of the gaze target tasks on these gains. The results showed no difference in gaze target tasks for gain ($t_{18} = -0.6, P = 0.545, d = 0.142$). We further examined this finding using a Bayesian paired *t* test, which indicated that the data were 3.552 times more likely under the null hypothesis than under the alternative, providing moderate evidence for the null hypothesis. Figure 4D presents the mean values for each participant across the two gaze-target tasks. The

mean value was 4.02 ± 0.39 N for the stationary gaze target, and 4.12 ± 0.45 N for the moving gaze target. Unlike the correction onset, there was a strong association between response gain for stationary and moving gaze targets ($r = 0.944, P < 0.001$; Fig. 4D).

DISCUSSION

The aim of the current study was to determine whether gaze-related signals involved in directing the hand movements

toward a target would be disrupted by an active oculomotor tracking task. Participants either fixated a stationary target or tracked a moving target while reaching to a spatially dissociated reach target. During the reach, we perturbed the hand, requiring participants to make rapid corrections. We found evidence that gain of reach corrections was not modulated by the oculomotor tracking task, whereas evidence for correction onset was inconclusive. Moreover, we found that response gains were strongly correlated across tasks, indicating consistent individual response profiles that were independent of the gaze-task manipulation. Although participants remained engaged in the smooth pursuit task, their pursuit performance slightly declined during reaching compared with the preparatory period.

Gaze-Related Signals When Reaching to Visual Targets

In the current study, participants successfully performed the secondary gaze task while reaching. When instructed to maintain fixation or pursue a moving target, they generally kept their gaze within the predefined boundary region, with occasional large saccades away from the gaze target. Across conditions, eye position error remained low, $\sim 1^\circ$, during the preparatory period, and increased modestly after movement onset. For the pursuit condition, eye-velocity gain was near 1 before reach onset and gradually declined to ~ 0.7 by the end of the movement. These changes indicate that participants remained engaged in the smooth pursuit task, but performance during reaching declined compared with the preparatory period.

When naturally reaching to an object or visually cued location, humans typically fixate the target location throughout the reaching movement, a visuomotor behavior that supports directing and guiding the hand toward the target (24). Previous work has shown that gaze-related signals—including proprioceptive signals from the eye and peripheral vision of the hand—support rapid, automatic corrections of movement errors when participants fixate on the reach target (2, 3, 16, 25, 26). Importantly, these rapid corrections also occur when participants fixate on a location dissociated from the current reach goal (11, 13, 14). Here, we show that corrections during goal-directed reaching are as fast and strong when participants—instead of fixating a stationary target—engage in an oculomotor tracking task, suggesting that continuous eye movements do not disrupt the use of gaze-related signals.

Classic work has shown that gaze-position-related signals can contribute to the spatial guidance of the hand. For example, Prablanc et al. (27) demonstrated that fixating a reach target improves endpoint accuracy even in the absence of visual feedback of the hand, consistent with the use of gaze position signals (proprioception and/or efference copy) in movement control. Building on this, Neggers and Bekkering (12, 28, 29) showed that when participants fixate a separate stationary gaze target while reaching to another location, gaze tends to remain “anchored” to the fixation target until the reach is completed (“gaze-locking”), even when the hand is not visible. This is consistent with the idea that gaze position signals can be used to help control the hand during ongoing reaching movements. Our current results indicate that during pursuit, peripheral vision can be used effectively

to correct for reach errors. However, it remains an open question whether the continuously changing gaze position signals generated during smooth pursuit of a gaze target can serve as a useful spatial reference to guide the hand to a separate reach target. One way to address this would be to extend Neggers and Bekkering’s task to a smooth pursuit context, in which participants pursue a moving target while reaching—without visual feedback of the hand—to a separate location and are required to shift gaze to a newly appearing stationary target during the reach.

Smooth Pursuit, Attention, and the Online Control of Reaching

Research on manual interception has shown that humans naturally track moving targets with smooth-pursuit eye movements (30). When participants pursue an unpredictably moving target and are then instructed to intercept it, they not only maintain pursuit after hand movement initiation but also tend to suppress catch-up saccades until the moment of contact (19). The suppression of these discrete eye jumps is thought to provide the manual system with a continuous, uninterrupted oculomotor signal to guide the hand. Indeed, research on interception tasks indicates that smooth pursuit provides a high-fidelity velocity signal that the brain uses to predict future object states. For example, during manual interception, the brain uses pursuit speed to scale anticipatory postural adjustments—stiffening the leg and trunk muscles in preparation for the force of impact before it actually occurs (31, 32). These results demonstrate that pursuit signals are normally “broadcast” across the motor system to coordinate the whole body for action. In this context, our finding that reach-correction gains are unaffected by pursuit is striking; it suggests that even when the pursuit system is actively broadcasting these large-scale motor signals, the specific feedback loop for manual reach corrections can operate in isolation.

Although the oculomotor system showed a slight performance decrement during the reach, this result is consistent with a general dual-task cost observed when smooth pursuit is paired with secondary cognitive or auditory tasks—conditions in which tracking performance is known to be sensitive to top-down attentional demands even when the secondary task is nonvisual in nature (33–35). Given these results, we should be cautious in suggesting that the specific visual demands linked to reach corrections influence pursuit performance, as the decrement may instead reflect the general attentional costs of performing a concurrent motor task.

Gain Put Not Correction Onset Is Correlated within Individuals

We found a within-participant correlation in feedback gain, but not in the onset of the correction, between the two visuomotor task conditions. These results are consistent with the idea that corrective feedback responses are initiated automatically—and as early as the processing hierarchy allows (36)—resulting in little variability across participants. At the same time, the gain of the response is known to be more sensitive to changes in visuomotor task demands (11, 17, 37) and thus it is not surprising it can also vary considerably across individuals. Similar to the feedback gain, we

found that hand movement kinematics, that is, movement onset, duration, and peak velocity, were highly correlated within participants across tasks, suggesting that individuals have preferred movement signatures.

Limitations

A limitation of the present study concerns the estimation of the correction onset. The relatively small number of perturbation trials may have increased variability in onset measurements across participants, potentially reducing sensitivity to small temporal differences. This limitation is likely less critical for estimates of feedback gain, which are generally more robust to trial-to-trial variability. In addition, although the channel stiffness and damping were sufficient to detect feedback responses, these parameters may not have been optimal for capturing subtle changes in feedback gain and, particularly, the precise timing of response onset. Therefore, onset-related findings should be interpreted with caution.

Conclusions

Our findings indicate that rapid, automatic visual feedback mechanisms that support reaching are equally strong during pursuit tracking and fixation of a separate gaze target. This indicates that the visuomotor processes that are engaged in smooth pursuit of a moving target, above and beyond those involved in fixating a stationary target, do not influence the reach-related visuomotor processes. Note that these conclusions are limited to the tasks examined here; further studies are needed to determine whether they generalize to more complex reaching tasks.

DATA AVAILABILITY

Source data for this study are openly available at <https://doi.org/10.17605/OSF.IO/DFGQ2>.

ACKNOWLEDGMENTS

The authors thank Martin York for technical support. Preprint is available at <https://doi.org/10.64898/2026.02.28.708705>.

GRANTS

This work was supported by a Deutsche Forschungsgemeinschaft (DFG) Research Fellowship under Grant No. FO 1347/1-1 (to J.F.), the Natural Sciences and Engineering Research Council of Canada Grant 156173 (to J.R.F.), the National Council for Scientific and Technological Development (CNPq, Brazil) Grant 304056/2022-7 (to R.M.), and the São Paulo Research Foundation (FAPESP, Brazil) Grant 2019/21749-6 (to R.M.).

DISCLOSURES

No conflicts of interest, financial or otherwise, are declared by the authors.

AUTHOR CONTRIBUTIONS

R.M., J.F., and J.R.F. conceived and designed research; R.M. performed experiments; R.M., J.F., and J.R.F. analyzed data; R.M., J.F., J.P.G., and J.R.F. interpreted results of experiments; R.M., J.F., and J.R.F. prepared figures; R.M. and J.F. drafted manuscript;

R.M., J.F., J.P.G., and J.R.F. edited and revised manuscript; R.M., J.F., J.P.G., and J.R.F. approved final version of manuscript.

REFERENCES

1. Goodale MA, Pelisson D, Prablanc C. Large adjustments in visually guided reaching do not depend on vision of the hand or perception of target displacement. *Nature* 320: 748–750, 1986. doi:10.1038/320748a0.
2. Paillard J. Fast and slow feedback loops for the visual correction of spatial errors in a pointing task: a reappraisal. *Can J Physiol Pharmacol* 74: 401–417, 1996. doi:10.1139/y96-033.
3. Saunders JA, Knill DC. Humans use continuous visual feedback from the hand to control fast reaching movements. *Exp Brain Res* 152: 341–352, 2003. doi:10.1007/s00221-003-1525-2.
4. Scott SH. Optimal feedback control and the neural basis of volitional motor control. *Nat Rev Neurosci* 5: 532–546, 2004. doi:10.1038/nrn1427.
5. Cluff T, Scott SH. Rapid feedback responses correlate with reach adaptation and properties of novel upper limb loads. *J Neurosci* 33: 15903–15914, 2013. doi:10.1523/JNEUROSCI.0263-13.2013.
6. Diedrichsen J. Optimal task-dependent changes of bimanual feedback control and adaptation. *Curr Biol* 17: 1675–1679, 2007. doi:10.1016/j.cub.2007.08.051.
7. Dimitriou M, Franklin DW, Wolpert DM. Task-dependent coordination of rapid bimanual motor responses. *J Neurophysiol* 107: 890–901, 2012. doi:10.1152/jn.00787.2011.
8. Franklin S, Wolpert DM, Franklin DW. Visuomotor feedback gains upregulate during the learning of novel dynamics. *J Neurophysiol* 108: 467–478, 2012. doi:10.1152/jn.01123.2011.
9. Gallivan JP, Logan L, Wolpert DM, Flanagan JR. Parallel specification of competing sensorimotor control policies for alternative action options. *Nat Neurosci* 19: 320–326, 2016. doi:10.1038/nn.4214.
10. de Brouwer AJ, Jarvis T, Gallivan JP, Flanagan JR. Parallel specification of visuomotor feedback gains during bimanual reaching to independent goals. *eNeuro* 4: ENEURO.0026-17.2017, 2017. doi:10.1523/ENEURO.0026-17.2017.
11. de Brouwer AJ, Gallivan JP, Flanagan JR. Visuomotor feedback gains are modulated by gaze position. *J Neurophysiol* 120: 2522–2531, 2018. doi:10.1152/jn.00182.2018.
12. Neggers SF, Bekkering H. Ocular gaze is anchored to the target of an ongoing pointing movement. *J Neurophysiol* 83: 639–651, 2000. doi:10.1152/jn.2000.83.2.639.
13. Reichenbach A, Franklin DW, Zlatka-Haas P, Diedrichsen J. A dedicated binding mechanism for the visual control of movement. *Curr Biol* 24: 780–785, 2014. doi:10.1016/j.cub.2014.02.030.
14. Franklin DW, Reichenbach A, Franklin S, Diedrichsen J. Temporal evolution of spatial computations for visuomotor control. *J Neurosci* 36: 2329–2341, 2016. doi:10.1523/JNEUROSCI.0052-15.2016.
15. Knill DC, Bondada A, Chhabra M. Flexible, task-dependent use of sensory feedback to control hand movements. *J Neurosci* 31: 1219–1237, 2011. doi:10.1523/JNEUROSCI.3522-09.2011.
16. Saunders JA, Knill DC. Visual feedback control of hand movements. *J Neurosci* 24: 3223–3234, 2004. doi:10.1523/JNEUROSCI.4319-03.2004.
17. Dimitriou M, Wolpert DM, Franklin DW. The temporal evolution of feedback gains rapidly update to task demands. *J Neurosci* 33: 10898–10909, 2013. doi:10.1523/JNEUROSCI.5669-12.2013.
18. Franklin DW, Wolpert DM. Specificity of reflex adaptation for task-relevant variability. *J Neurosci* 28: 14165–14175, 2008. doi:10.1523/JNEUROSCI.4406-08.2008.
19. Mrotek LA, Soechting JF. Target interception: hand-eye coordination and strategies. *J Neurosci* 27: 7297–7309, 2007. doi:10.1523/JNEUROSCI.2046-07.2007.
20. Soechting JF, Rao HM, Juvelí JZ. Incorporating prediction in models for two-dimensional smooth pursuit. *PLoS One* 5: e12574, 2010. doi:10.1371/journal.pone.0012574.
21. Danion FR, Flanagan JR. Different gaze strategies during eye versus hand tracking of a moving target. *Sci Rep* 8: 10059, 2018. doi:10.1038/s41598-018-28434-6.
22. Fookien J, Moraes R, Scott AM, Flanagan JR. Microsaccadic modulation in goal-directed reaching. *J Vis* 26: 4, 2026. doi:10.1167/jov.26.3.4.

23. **JASP Team.** JASP (Version 0.17.3). Amsterdam, The Netherlands: JASP Team, 2023. <https://jasp-stats.org/>.
24. **Land MF, Mennie N, Rusted J.** The roles of vision and eye movements in the control of activities of daily living. *Perception* 28: 1311–1328, 1999. doi:10.1068/p2935.
25. **Brenner E, Smeets JBJ.** Fast responses of the human hand to changes in target position. *J Mot Behav* 29: 297–310, 1997. doi:10.1080/00222899709600017.
26. **Sarlegna F, Blouin J, Bresciani JP, Bourdin C, Vercher JL, Gauthier GM.** Target and hand position information in the online control of goal-directed arm movements. *Exp Brain Res* 151: 524–535, 2003. doi:10.1007/s00221-003-1504-7.
27. **Prablanc C, Pélisson D, Goodale MA.** Visual control of reaching movements without vision of the limb. I. Role of retinal feedback of target position in guiding the hand. *Exp Brain Res* 62: 293–302, 1986. doi:10.1007/BF00238848.
28. **Neggers SFW, Bekkering H.** Coordinated control of eye and hand movements in dynamic reaching. *Hum Mov Sci* 21: 349–376, 2002. doi:10.1016/s0167-9457(02)00120-3.
29. **Neggers SFW, Bekkering H.** Gaze anchoring to a pointing target is present during the entire pointing movement and is driven by a non-visual signal. *J Neurophysiol* 86: 961–970, 2001. doi:10.1152/jn.2001.86.2.961.
30. **Fooken J, Kreyenmeier P, Spering M.** The role of eye movements in manual interception: a mini-review. *Vision Res* 183: 81–90, 2021. doi:10.1016/j.visres.2021.02.007.
31. **Sinha O, Rosenquist T, Fedorshak A, Kpankpa J, Albenze E, T Bonnet C, Bertuccio M, Kurtzer I, Singh T.** Predictive posture stabilization before contact with moving objects: equivalence of smooth pursuit tracking and peripheral vision. *J Neurophysiol* 132: 695–709, 2024. doi:10.1152/jn.00158.2024.
32. **Sinha O, Muttee AP, Wu JH, Bertuccio M, Kurtzer I, Singh T.** Smooth pursuit eye movements contribute to long-latency reflex modulation in the lower extremity. *J Neurophysiol* 134: 998–1006, 2025. doi:10.1152/jn.00023.2025.
33. **Hutton SB, Tegally D.** The effects of dividing attention on smooth pursuit eye tracking. *Exp Brain Res* 163: 306–313, 2005. doi:10.1007/s00221-004-2171-z.
34. **Kathmann N, Hochrein A, Uwer R.** Effects of dual task demands on the accuracy of smooth pursuit eye movements. *Psychophysiology* 36: 158–163, 1999. doi:10.1111/1469-8986.3620158.
35. **Lovejoy LP, Fowler GA, Krauzlis RJ.** Spatial allocation of attention during smooth pursuit eye movements. *Vision Res* 49: 1275–1285, 2009. doi:10.1016/j.visres.2009.01.011.
36. **Scott SH.** A functional taxonomy of bottom-up sensory feedback processing for motor actions. *Trends Neurosci* 39: 512–526, 2016. doi:10.1016/j.tins.2016.06.001.
37. **Pruszynski JA, Omrani M, Scott SH.** Goal-dependent modulation of fast feedback responses in primary motor cortex. *J Neurosci* 34: 4608–4617, 2014. doi:10.1523/JNEUROSCI.4520-13.2014.